Evidence for adaptive functional changes in the cerebral cortex with axonal injury from multiple sclerosis

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Summary
Axonal injury occurs even in the earliest stages of multiple sclerosis. Magnetic resonance spectroscopic imaging (MRSI) measurements of brain N-acetylaspartate (NAA), a marker of axonal integrity, show that this axonal injury can occur even in the absence of clinically evident functional impairments. To test whether cortical adaptive responses contribute to the maintenance of normal motor function in patients with multiple sclerosis, we performed MRSI and functional MRI (fMRI) examinations of nine multiple sclerosis patients who had unimpaired hand function. We found that activation of the ipsilateral sensorimotor cortex with simple hand movements was increased by a mean of fivefold relative to normal controls (n = 8) and that the extent of this increase was strongly correlated (σ = −0.93, P = 0.001) with decreases in brain NAA. These results suggest that compensatory cortical adaptive responses may help to account for the limited relationship between conventional MRI measures of lesion burden and clinical measures of disability, and that therapies directed towards promoting cortical reorganization in response to brain injury could enhance recovery from relapses of multiple sclerosis.

Keywords: fMRI; multiple sclerosis; brain; rehabilitation; recovery

Abbreviations: Cr = creatine; fMRI = functional magnetic resonance imaging; LI = lateralization index; MRSI = magnetic resonance spectroscopic imaging; NAA = N-acetylaspartate; SMA = supplementary motor cortex; SMC = sensorimotor cortex; TE = echo time; TR = repetition time

Introduction
Multiple mechanisms have been postulated to contribute to maintenance of function after inflammatory brain injury in multiple sclerosis. These include resolution of the acute inflammation, remyelination (Lassmann et al., 1997) and increased expression of sodium channels in chronically demyelinated segments of axons (Waxman and Ritchie, 1993). However, magnetic resonance spectroscopic imaging (MRSI) studies of multiple sclerosis patients have emphasized that considerable axonal injury occurs even within acute plaques (Arnold et al., 1990, 1998). Whereas there can be some degree of reversible axonal injury (De Stefano et al., 1995b), direct pathological studies have confirmed that a substantial amount of the axonal injury and loss in plaques and in the normal appearing white matter appears irreversible (Ferguson et al., 1997; Trapp et al., 1998). None of the mechanisms of recovery noted above could be expected to contribute to the resolution of functional deficits resulting from such irreversible axonal injury or loss.

A clue to ways in which function may be preserved even when there is substantial axonal injury comes from experimental paradigms that have demonstrated a considerable capacity for cortical adaptation even in the adult brain (Witte, 1998). These cortical ‘plastic’ changes can involve local synaptic reorganization, reorganization at more distant sites (e.g. in subcortical nuclei projecting onto the cortex) or recruitment of parallel existing pathways. PET and functional MRI (fMRI) studies of patients who have recovered from stroke, or who maintain motor functions despite the
progressive enlargement of brain tumours compressing eloquent areas of cortex, have provided evidence that cortical plasticity may contribute to functional recovery after different forms of brain injury in man (Weiller et al., 1993; Chollet and Weiller, 1994; Cramer et al., 1997; Cao et al., 1998). A longitudinal case study of a patient with a relapse of multiple sclerosis has suggested a dynamic relationship between similar changes in cortical activation with movement and the extent of pathological changes (Reddy et al., 2000). A larger cross-sectional study of multiple sclerosis patients with a wide range of disabilities demonstrated altered patterns of cortical activation for motor tasks, suggesting both that both local and long distance changes occur in proportion to the lesion burden (Lee et al., 2000). Increased ipsilateral motor cortex activation (leading to decreased hemispheric lateralization of motor activation) was associated with an increasing burden of disease. However, this study did not control for performance differences between the subjects. Also, with the exception of the case study (Reddy et al., 2000), neither this nor previous studies of similar phenomena (Weiller et al., 1993; Chollet and Weiller, 1994; Cramer et al., 1997; Cao et al., 1998) directly assessed the neuronal and axonal injury likely to be responsible for driving reorganization, relying instead on less specific measures of the extent of pathological change.

We wished to test the hypothesis that cortical adaptive changes contribute to sustaining motor functions with the progression of axonal injury in multiple sclerosis more directly. We appreciated that it is difficult to interpret the significance of abnormal patterns of activation in functional imaging studies in patients if there are substantial differences in performance between the control and patient groups. Therefore, we chose to study motor cortex activation in a group of patients with relapsing remitting multiple sclerosis who had normal finger tapping ability. In this group, we included primary sensorimotor plus premotor cortex from anatomical landmarks. The sensorimotor cortex (SMC) was defined as the area medial to this. A lateralization index (LI) was defined as \( \frac{C - 2I}{C + I} \) where \( C \) is the number of significantly activated voxels in the contralateral SMC and \( I \) is the number of significantly activated pixels in the ipsilateral SMC.

### Methods

#### Patients

Patients were selected from the out-patient population of the Montreal Neurological Institute. Normal controls (eight right-handed) were volunteers recruited from hospital and research staff. Only five of the controls had both fMRI and MRSI studies. All gave informed consent for the protocol, which was approved by the ethics committee of the Montreal Neurological Institute. Finger tapping rates for all of the patients (six right-handed, three left-handed) were equal to or better than performance for the normal controls (4.5 ± 0.6 Hz).

#### fMRI

The motor task involved simultaneous four-finger flexion–extension of the metacarpal-phalangeal joints of the dominant hand paced by an auditory cue at 75% of the maximum rate (~3 Hz) for each subject. This was alternated with rest (during which time the auditory cue continued). All subjects were visually monitored during the experiment to ensure compliance with the protocol. Data was acquired with a 1.5 T Siemens Magnetom Vision [gradient echo planning, repetition time (TR) = 4 s, echo time (TE) = 47 ms, field of vision = 320 × 320, 64 × 64 matrix, slice thickness 6 mm]. A total of 120 volumes were obtained for each hand in a trial with alternating blocks of rest or movement, during which 20 volumes were acquired for each block. Two trials were performed for movements of each hand. In the analysis, data from the two trials for each hand were concatenated. Image processing and statistical analysis were carried out using a locally (Oxford FMRI Centre) extended version of MEDx 3.0 (Sensor Systems, Inc., Sterling, Va., USA). Motion correction, spatial smoothing (full width half maximum = 5 mm), intensity normalization and temporal filtering were applied. Activation maps were calculated using Student’s unpaired \( t \)-test, and cluster detection (Poline et al., 1997) was performed on all voxels above \( Z = 6.0 \) to determine clusters significantly activated (\( P < 0.01 \)). The functional image was registered to the structural image and the resulting transform applied to the activation map, which was then overlaid on a high resolution \( T_1 \) structural image for neuroanatomical correlation of the activations.

Motor cortex was defined on the structural image using anatomical landmarks. The sensorimotor cortex (SMC) included primary sensorimotor plus premotor cortex from the region within the lateral post-central gyrus anteriorly to the point midway between the central sulcus and the anterior limit of the brain. The supplementary motor area (SMA) was defined as the area medial to this. A lateralization index (LI) was defined as \( C - 2I/C + I \) where \( C \) is the number of significantly activated voxels in the contralateral SMC and \( I \) is the number of significantly activated pixels in the ipsilateral SMC.

#### MRSI and MRI

Conventional proton MRI and MRSI examinations of the brain were performed together using a Philips Gyroscan ACS II at 1.5 T. Anatomical images were acquired using a dual turbo spin-echo sequence (TR = 2075 ms, TE = 30/90 ms, slice thickness = 3 mm) producing proton density weighted and \( T_2 \)-weighted images. These transverse images were used to select a volume of interest for spectroscopy of ~ 90 × 90 × 20 mm centred on the corpus callosum. Water-suppressed proton spectra were acquired using a 90-180-180 (PRESS) sequence (TR = 2 s, TE = 272 ms, 32 × 32 phase-encodes and 250 mm field of view). To allow for correction of \( B_0 \) inhomogeneity during post-processing, a
Table 1 Clinical data describing patients and individual levels of disability

<table>
<thead>
<tr>
<th>Patient</th>
<th>T2 LV (cm)</th>
<th>EDSS</th>
<th>Dominant hand</th>
<th>Maximum finger tapping rate (Hz)</th>
<th>Disease duration (years)</th>
<th>Type of multiple sclerosis</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>9.4</td>
<td>2</td>
<td>L</td>
<td>6.0</td>
<td>3.4</td>
<td>RR</td>
</tr>
<tr>
<td>2</td>
<td>20.5</td>
<td>5</td>
<td>R</td>
<td>3.4</td>
<td>3.3</td>
<td>SP</td>
</tr>
<tr>
<td>3</td>
<td>24.9</td>
<td>3</td>
<td>R</td>
<td>4.6</td>
<td>23.2</td>
<td>RR</td>
</tr>
<tr>
<td>4</td>
<td>3.2</td>
<td>3.5</td>
<td>R</td>
<td>4.4</td>
<td>11.6</td>
<td>RR</td>
</tr>
<tr>
<td>5</td>
<td>13.5</td>
<td>6.5</td>
<td>L</td>
<td>3.1</td>
<td>12.5</td>
<td>SP</td>
</tr>
<tr>
<td>6</td>
<td>4.9</td>
<td>3</td>
<td>R</td>
<td>4.8</td>
<td>10.7</td>
<td>RR</td>
</tr>
<tr>
<td>7</td>
<td>1.2</td>
<td>2</td>
<td>L</td>
<td>5.6</td>
<td>17.5</td>
<td>RR</td>
</tr>
<tr>
<td>8</td>
<td>4.8</td>
<td>2.5</td>
<td>R</td>
<td>3.8</td>
<td>23.0</td>
<td>RR</td>
</tr>
<tr>
<td>9</td>
<td>0.4</td>
<td>0</td>
<td>R</td>
<td>7.8</td>
<td>6.8</td>
<td>RR</td>
</tr>
</tbody>
</table>

Median: 9.2, 3, 4.6, 11.6
Range: 0.4–29.7, 0–6.5, 3.1–7.8, 3.3–23.2

Abbreviations: T2 LV = lesion volume on T2-weighted MRI scan; NAA/Cr = ratio of N-acetylaspartate to creatine in magnetic resonance spectrum from defined volume; EDSS = Expanded Disability Status Scale; RR = relapsing–remitting; SP = secondary progressive. The maximum finger tapping rate was measured as described in Methods and is reported for the dominant hand only.

Results

The patients had either relapsing-remitting (n = 7) or secondary progressive (n = 2) multiple sclerosis (Table 1). None had suffered a relapse more recently than 4 months before the study. While disability varied substantially (median Extended Disability Status Scale 3.0; range 0–6.5), all patients were without motor or sensory symptoms in the arms or hands and showed maximum finger tapping rates with the dominant hand that were as fast as (or faster than) those in the normal control group. No mirror movements were noted during tapping of either the left or right hands in the patient or control groups.

The patients had a mean lesion volume of 10.3 cm³ measured on the T2-weighted MRI (range, 0.4–24.9 cm³). There was only a trend for a reduction in the mean relative cerebral white matter NAA concentration (P = 0.08) measured by MRSI in this mildly affected group of multiple sclerosis patients relative to the normal controls (relative NAA/Cr patient mean, n = 9, 2.99 ± 0.32; normal controls, n = 5, 3.26 ± 0.16, which is in good agreement with values for our larger group of normal controls, n = 27, 3.21 ± 0.21).

With movement of the dominant hand, both the normal controls (n = 8, right handed) and patients (n = 9, six right-handed, three left-handed) showed significant activations in the SMA and in the contralateral and ipsilateral SMC (Fig. 1). The smaller volumes (see below) of ipsilateral SMC activations for the control subjects were localized somewhat variably in the precentral gyrus and posterior middle frontal gyrus, while the rather greater activation in this region for the patients tended to be centred in the precentral gyrus. fMRI activation images during the hand movement task showed similar mean maximum Z scores (Zmax) in each of the regions studied (for patients and controls together, n = 17: contralateral SMC, Zmax = 12.2 ± 1.6; ipsilateral SMC, Zmax = 6.4 ± 3.9; SMA, Zmax = 8.5 ± 3.9).

The relative hemispheric LI of cortical activation during this motor task was lower for the patients as a group than for the controls (P < 0.02) (Table 2). There was a strong correlation between the LI and the relative brain NAA for the patients (σ = 0.80, P = 0.009) and for the group as a whole (σ = 0.73, P = 0.003) (Fig. 2A). This correlation arose primarily from increases in ipsilateral motor cortex activation with lower values of brain NAA (for patients alone, σ = −0.93, P = 0.001; for the group as a whole, σ = −0.70, P = 0.006) (Fig. 2B). Both relationships remained significant if only right-handed patients were considered in the total group (correlation of NAA/Cr with LI, σ = 0.65,
Adaptive functional changes with axonal injury

Fig. 1 Representative activation maps registered on single-shot echo planar MRIs from a normal control (A), a multiple sclerosis patient with a higher, normal range NAA/creatine concentration ratio in the cerebral white matter and normal range ipsilateral motor cortex activation (B), and a multiple sclerosis patient with a NAA/creatine concentration ratio in cerebral white matter below the normal range showing a relatively larger activation in ipsilateral motor cortex (C). As described previously (Lee et al., 2000), patients may sometimes show relatively increased activation of the supplementary motor/premotor areas as in C, although we did not find this difference significant for the group as a whole.

Table 2 Activations in contra- and ipsilateral SMC and SMA with calculated hemispheric LI and related lesion volume for each patient, and a comparison with normal controls

<table>
<thead>
<tr>
<th>Patient</th>
<th>NAA/Cr</th>
<th>Numbers of pixels above threshold</th>
<th>Total</th>
<th>LI</th>
<th>Lesion volume (cm³)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Contralateral</td>
<td>Ipsilateral</td>
<td>SMA</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>SMC</td>
<td>SMC</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>1</td>
<td>2.56</td>
<td>98.0</td>
<td>32.0</td>
<td>6.0</td>
<td>136.0</td>
</tr>
<tr>
<td>2</td>
<td>2.73</td>
<td>213.0</td>
<td>79.0</td>
<td>97.0</td>
<td>389.0</td>
</tr>
<tr>
<td>3</td>
<td>2.72</td>
<td>94.0</td>
<td>18.0</td>
<td>3.0</td>
<td>115.0</td>
</tr>
<tr>
<td>4</td>
<td>2.93</td>
<td>53.0</td>
<td>16.0</td>
<td>12.0</td>
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</tr>
<tr>
<td>5</td>
<td>2.88</td>
<td>80.0</td>
<td>17.0</td>
<td>60.0</td>
<td>157.0</td>
</tr>
<tr>
<td>6</td>
<td>3.13</td>
<td>64.0</td>
<td>12.0</td>
<td>47.0</td>
<td>123.0</td>
</tr>
<tr>
<td>7</td>
<td>3.16</td>
<td>34.0</td>
<td>1.0</td>
<td>0.0</td>
<td>35.0</td>
</tr>
<tr>
<td>8</td>
<td>3.23</td>
<td>99.0</td>
<td>5.0</td>
<td>40.0</td>
<td>144.0</td>
</tr>
<tr>
<td>9</td>
<td>3.59</td>
<td>55.00</td>
<td>0.0</td>
<td>11.0</td>
<td>66.0</td>
</tr>
<tr>
<td>Mean ± SD</td>
<td>2.99 ± 0.32</td>
<td>87.8 ± 52.1</td>
<td>20.0 ± 24.3</td>
<td>30.7 ± 31.0</td>
<td>138.4 ± 96.2</td>
</tr>
<tr>
<td>Control (mean ± SD) (n = 8)</td>
<td>3.26 ± 0.16</td>
<td>110.9 ± 10.3</td>
<td>3.8 ± 4.2</td>
<td>23.4 ± 20.4</td>
<td>138.0 ± 29.7</td>
</tr>
</tbody>
</table>

The extent of activation in each region of interest is expressed as the number of pixels above the chosen threshold (see Methods). *
P < 0.02.
Patients (2 and 6). The increase in range was due to activation that was more than twice as large as for the controls (Matthews et al., 1998). Another important feature of the experimental design for the current work is that the choice of patients with normal fine-finger movements removed performance differences as a confound to interpretation. We therefore interpret the cortical activation changes as evidence for adaptive responses that may act to maintain normal functional capacity after axonal injury associated with the inflammatory lesions of multiple sclerosis. This phenomenon may contribute to limiting the strength of the relationship between disability and measures of multiple sclerosis pathology (e.g., MRI lesion burden) (Filippi et al., 1998).

The major difference in the pattern of cortical motor activation seen in the patient group was a greater activation of ipsilateral SMC with greater degrees of axonal injury (as assessed from decreases in relative NAA measured by MRSI). There was no clinical evidence for ‘mirror’ movements of the opposite hand to account for this and such movements are uncommon in subjects without paresis. EMG documentation showing that there is no muscle activity in the arm at rest would be desirable in further studies, particularly if the subjects have some degree of weakness. However, the observation of ipsilateral SMC activation itself is perhaps not so surprising, as ipsilateral SMC activity is observed in normal subjects with respect to increasing task complexity or rate (Wexler et al., 1997a). Brains of patients with multiple sclerosis may use similar mechanisms to maintain normal performance levels with increasing injury in the brain. We suggest therefore that these changes represent an ‘unmasking’ of existing motor pathways in the multiple sclerosis patients rather than novel cortical reorganization occurring in response to axonal injury or other specific factors associated with the disease.

Functional recovery in multiple sclerosis has previously been recognized to occur through a variety of mechanisms including resolution of inflammatory changes, remyelination and reorganization of axonal membrane ion channels. A degree of axonal injury appears to be reversible (De Stefano et al., 1995b), although fixed, irreversible axonal injury also occurs even in acute multiple sclerosis lesions (De Stefano et al., 1995a; Ferguson et al., 1997; Trapp et al., 1998; Evangelou et al., 2000). On the basis of this study we speculate that cortical adaptive changes could also contribute to functional recovery from lesions causing irreversible axonal injury.
One concern in interpretation was that the failure to balance handedness between the control and patient groups might bias results, as left-handed subjects have been reported to have an ~30% lower hemispheric lateralization of motor cortex activation than right-handed subjects for a serial finger opposition task with the dominant hand (Kim et al., 1993). Relative lateralization of activation depends on task complexity, however (Wexler et al., 1997b). In preliminary studies [performed using a 3 T MRI system (Lee et al., 2000), which gives an overall lower apparent lateralization of activation than in the current study because of greater sensitivity to the lower ipsilateral SMC activations], we found only an ~10% difference for this simple hand-tapping task performed by the dominant hand (mean LI = 0.55 ± 0.28, left dominant, n = 5; mean LI = 0.61 ± 0.39, right dominant, n = 14; R. Pineiro, S. Pendlebury, H. Johansen-Berg and P. M. Matthews, unpublished data). This difference could not explain the 44% decrease in LI for Patient 1, for example. Furthermore, as described in Results, a significant correlation (although somewhat weaker than for the group as a whole) is found between decreasing NAA/Cr and LI even if left-handed patients are excluded from the analysis.

We did not observe a significant posterior shift in the localization of contralateral SMC activations as reported in our earlier study of patients with a higher burden of disease and upper limb disability (Lee et al., 2000). This activation localization shift was hypothesized to arise from local cortical reorganization in the patients. In the current study, only the SMC activation centres for Patients 2 and 6 were >2 SD posterior to the normal control mean. The failure to observe a significant shift for the group as a whole may be a consequence of the lack of disease burden sufficient to cause significant disability in fine finger movements for this group. This suggests that if a local posterior shift in the centre of SMC activation is part of adaptive responses to injury, then it may occur only with more severe injury than is necessary to enhance ipsilateral SMC activation.

We believe that measurements of the relative NAA concentrations in the central white matter as performed for this study are relevant to understanding functional changes in the corticospinal tract, even though this region was not selectively sampled. Axonal injury occurs throughout the normal appearing white matter (Narayanan et al., 1997). This injury pattern shows only modest regional variation on average (although it is greatest in the periventricular region) (Narayanan et al., 1997). While it is uncertain whether the decreases in the NAA/Cr are due solely to decreases in NAA, there is no doubt but that (i) the absolute NAA concentration decreases in the white matter of multiple sclerosis patients (Sarchielli et al., 1999); (ii) substantial axonal loss occurs in the white matter, consistent with the decreases in NAA/Cr in patients (Evangelou et al., 2000); and (iii) lower NAA/Cr is associated with greater disability (Fu et al., 1998).

The absolute number of activated voxels is a function of the statistical threshold chosen. Use of Z > 6.0 (P < 0.0003) gave similar degrees of activation in patients and controls and suppressed artefactual (e.g. from subject motion) activations during the movement paradigm. In separate studies, we have shown that detection of changes in LI is relatively insensitive to the precise Z threshold chosen, although the precise value of the LI varies as the threshold changes (H. Johanssen-Berg, R. Pineiro and P. M. Matthews, unpublished results). In the present case, both patients and controls were highly cooperative and the absolute activations were very similar between the two groups, justifying use of a single threshold level in the comparisons.

It also has been noted that measurement of percentage signal change may provide the most robust measure of activation (Cohen and DuBois, 1999). However, in a separate experiment we compared the relative LI for this hand-tapping protocol measured using the thresholded mean difference image with that from the thresholded Z score image for patients after strokes and for normal controls. We found no meaningful differences between the measures (R. Pineiro and P. M. Matthews, unpublished). Consequently, we have continued to use the thresholded Z score image for measures of the extent (as opposed to the magnitude) of the regional activation.

Overall, our results suggest that the cortical adaptive responses may have an important role in compensating for axonal injury in multiple sclerosis. We therefore propose that loss of adaptive capacity of the cortex with progression of axonal loss in multiple sclerosis could contribute to the development of progressive disease and the accumulation of irreversible clinical deficits. If this is true, then neurotrophic factors or other agents that promote neuronal ‘plasticity’ could promote improved functional recovery or slow progression of the disease.

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References


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